

A PMUT Integrated Microfluidic System for Volumetric Flow Rate Sensing

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Outline

- 1. Introduction
- 2. Fabrication
- 3. Working Principle
- 4. Experimental Setup
- 5. Results
- 6. Conclusion

1. INTRODUCTION

3

Introduction

- Volume flow rate is one of the ways to quantitatively characterize fluid flow
- It is the volume of a fluid that passes a known spatial coordinate per unit time
- Fluid density-dependent resonant frequency shift is the method for measuring volume flow rate described in the paper

4

2. FABRICATION

Fabrication

- The PMUT uses PZT as the piezoelectric material (deposited using sol-gel method)
- Contains one driving and one sensing electrode
- Fabricated on an SOI substrate
- Made in a circular shape



Figure 1: A cross-sectioned 3D schematic of single cell dual-electrode PMUT showing consisting layers

Integration with Microfluidics

- 1. Silicon wafer patterned using photoresist then etched using DRIE
- 2. The structure obtained is used as a mold
- 3. PDMS and curing compound mixture (10:1) poured over the mold, cured for 1 hour (120°C)
- 4. PDMS stripped off and 1mm diameter holes punched for inlet and outlet
- 5. Microfluidic channel and PMUT cell array aligned and bonded



Figure 2: The PMUT-Microfluidic-Integration



3. WORKING PRINCIPLE

Working Principle

- Works by virtual added mass effect
- Fluid pushed into inlet via a syringe pump (constant flow rate)
- Air-fluid interface created inside microfluid channel
- Virtual added mass created as air-fluid interface touches and moves on PMUT surface
- The RF value lowers, then reaches a constant value once the PMUT is fully covered
- Time taken for the RF to reach this value is the Resonant Switch Time (RST)

Flow rate (Q) = $\frac{\varphi * s}{RST}$

where,

 φ is the diameter of the PMUT, and s is the microfluidic channel cross-section

4. EXPERIMENTAL SETUP

Experimental Setup

- Device die bonded to custom made PCB
- Electrical isolation of the PMUT from the fluid achieved by using a Teflon solution (cured at 60°C, 2 hours)
- Connected to syringe pump
- LDV used to observe the frequency response of the PMUT



Figure 3: A PMUT-Microfluidic-Integration wirebonded to a custom-made printed circuit board



Figure 4: The experimental arrangement used for microfluidic flow sensing

5. RESULTS

Results

- Deionized water used for testing (syringe pump rate of 50 µl/hr)
- Air-fluid interface forms a nearly vertical line
- Resonant freq of single cell in PMUT array tracked and recorded using LDV
- Frequency of the device shifts relative to the air-fluid interface
- Time taken from in-air frequency value to in-fluid value is directly proportional to interface crossing time



Figure 5: Frequency response function obtained using the MSA 500, Laser Doppler Vibrometer (LDV), as the air-fluid interface flows along the PMUT in (a) 22.75 s (b) 33.28 s (c) 42 s

Actual vs Sensed Rate

- Varied flow rates from 30 µl/hr to 50 µl/hr
- time taken for the frequency to switch was recorded
- Flow rate calculated using previous equation
- Data plotted
- Slope value of 1.04 confirms negligible difference in actual and sensed values





Flow Sensitivity

- RST recorded for same range of flow rates
- Plot of RST vs flow rate
- Slope of line gives the sensitivity of the device
- Sensitivity found to be 537 ms/µl/hr



Figure 7: Graph showing the variation in the resonant shift time with respect to varying flow rates

6. CONCLUSION

Conclusion

- Dual-electrode PMUTs were developed for flow rate sensing
- The module was used along with a novel technique for measuring volumetric flow rate
- The technique was based on resonant frequency shift

Thank You!

Q&A

Additional Info

MATERIAL	ELECTRICAL CONDUCTIVITY
	Silver
Copper	64.1×10^{6}
Gold	49.0×10^{6}
Aluminium	40.8×10^{6}
Rhodium	23.3×10^{6}
Zinc	18.2×10^{6}
Nickel	16.4×10^{6}
Cadmium	14.7×10^{6}
Iron	11.2×10^{6}
Platinum	10.2×10^{6}
Palladium	9.3×10^{6}
Tin	8.7×10^{6}
Chromium	7.9×10^{6}
Lead	5.3×10^{6}
Titanium	2.3×10^{6}
Mercury	1.0×10^{6}



INCREASING HARDNESS ACCORDING TO MOH'S SCALE

COBALT

ENAMEL STEEL

PLATINUM SILVER FINE GOLD

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10

